Rehabilitative ultrasound imaging for the assessment of selected morphometric parameters of the flexor hallucis longus muscle in healthy individuals: An inter- and intrarater reliability study

Туре

Research paper

Keywords

ultrasound, reliability, flexor hallucis longus, rater

Abstract

Introduction

Ultrasound imaging (USI) is useful to evaluate structures of the foot to guide treatment, but the reliability of USI technique needs to be clarified. The goal of the study was to evaluate the intra- and inter-examiner reliability of USI image capture, and measurement of the cross-sectional area (CSA) and thickness of the flexor hallucis longus (FHL) for experienced and novice examiners

Material and methods

FHL images were captured for 20 healthy adults. Reliability of image capture was evaluated between images repeated at 10-min interval for an experienced and a novice examiner. Reliability of imagebased measurements was evaluated for one experienced and one novice rater, using all images. The intra-class correlation coefficient (ICC) and the standard error of measurement (SEM) were calculated

Results

Intra-examiner reliability of image capture for the FHL muscle examined by USI was excellent for both thickness (ICC3,1, 0.944–0.976; SEM, 6.8%–10.0%) and CSA (ICC3,1, 0.954–0.979; SEM, 10.8%–16.5%), with no effect of examiner experience. Reliability was also excellent for measurement of thickness (ICC3,1, 0.954–0.972; SEM, 1.2%–9.6%) and CSA (ICC3,1, 0.961–0.986; SEM, 9.2%–14.1%), with no effects of experience.

Conclusions

Reliability of image capture and image-based measurements developed by USI of CSA and thickness for the FHL muscle in healthy individuals was excellent, independent of the examiner experience.

Rehabilitative ultrasound imaging for the assessment of selected morphometric
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 intra- rater reliability study

Abstract: Background: Ultrasound imaging (USI) is useful to evaluate structures of the 4 foot to guide treatment, but the reliability of USI technique needs to be clarified. The goal 5 6 of the study was to evaluate the intra- and inter-examiner reliability of USI image capture, 7 and measurement of the cross-sectional area (CSA) and thickness of the flexor hallucis 8 longus (FHL) for experienced and novice examiners. Methods: FHL images were captured 9 for 20 healthy adults. Reliability of image capture was evaluated between images repeated 10 at 10-min interval for an experienced and a novice examiner. Reliability of image-based 11 measurements was evaluated for one experienced and one novice rater, using all images. 12 The intra-class correlation coefficient (ICC) and the standard error of measurement (SEM) 13 were calculated. Results: Intra-examiner reliability of image capture was excellent for both thickness (ICC_{3.1}, 0.944–0.976; SEM, 6.8%–10.0%) and CSA (ICC_{3.1}, 0.954–0.979; SEM, 14 15 10.8%–16.5%), with no effect of examiner experience. Reliability was also excellent for measurement of thickness (ICC_{3.1}, 0.954–0.972; SEM, 1.2%–9.6%) and CSA (ICC_{3.1}, 16 17 0.961–0.986; SEM, 9.2%–14.1%), with no effects of experience. Conclusion: Reliability of image capture and image-based measurements of CSA and thickness for the FHL muscle in 18 19 healthy individuals was excellent, independent of the examiner experience.

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- 21 Keywords: flexor hallucis longus, rater, reliability, ultrasound
- 22 Level of evidence: II.b
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30 Introduction

The flexor hallucis longus is the primary plantar flexor of the first metatarsophalangeal (MTP) and interphalangeal (IP) joints of the great toe; it also restrains the passive dorsiflexion at the first MTP joint and contributes to ankle plantar flexion [1]. FHL tendinopathy is one of the most common pathological conditions of the ankle and foot among active people [2].

Ultrasound imaging (USI) is considered as a safe, non-invasive, and valid method to measure muscle morphology to inform diagnosis, and to compare the cross-sectional area (CSA) and thickness of the FHL in healthy subjects [3], subjects with pes planus [4,5], and dancers [6]. Extending the application of USI in clinical practice would require assessing the reliability of measurements obtained.

41 Mickleet al. [7] evaluated the intra-examiner reliability of USI to measure the 42 morphology of the primary toe flexor muscles, while Crofts et al. [8] analyzed the inter-43 examiner reliability of USI for selected foot structures. Both of these studies suggest that USI 44 offers the opportunity to quantify the structures of the foot for a better understanding of their 45 functional contribution. Researchers have identified the need for determining the reliability 46 of USI not only for measurement (USI-based calculation) but also for image capture (patient 47 positioning), both of which might be influenced by the experience of the examiner. Valera-48 Calero et al. [9] have previously investigated the reliability of US image capture and 49 measurement of the CSA of the cervical multifidus muscle as a function of the examiner's 50 experience in asymptomatic individuals, with excellent reliability reported.

The objective of this study was to determine intra- and inter-examiner reliability of US image capture (probe assessment/subject positioning) and measurement (scan/image assessment) for the CSA and thickness of the FHL as a function of the examiner's experience. Understanding the architecture of the FHL has implications for invasive physiotherapeutic therapies, as most of them use ultrasound guidance to guarantee accuracy [10,11].

56 Materials and Methods

57 Participants

58 Twenty healthy volunteers were recruited from private physiotherapy clinics between 59 April and May 2020. The procedures were approved by the local Ethics Committee (1046-60 N-19) in accordance with the current national and international laws and regulations 61 governing the use of human subjects. Before participating in the study, the subjectss were fully informed about the protocol and written informed consent was obtained from each participant before testing. Enrolled participants were females over the age of 18 years and with no history of ankle pain over the previous year. The exclusion criteria were as follows: acute lower limb injury within the previous six months; prior ankle surgery; history of low back pain; history of peripheral nerve impairment; congenital/acquired foot deformities; any other medical condition or treatment affecting muscle tone.

68 Imaging capturing and FHL measurement protocol

69 For ultrasound evaluation of the FHL muscle, the participants lay in the prone position, 70 with the feet unsupported at the edge of the bed. The prone position is normally used for 71 invasive treatment techniques [10,11]. Using a previously described procedure [10,11], the 72 FHL muscle was located at the midpoint of the distance between the fibular head and the 73 inferior border of the lateral malleolus on the posterior aspect of the fibula, using the Logiq 74 US machine (GE Healthcare, USA; Fig 1). Images were captured using a 12 MHz linear 75 transducer, in the longitudinal and transverse plane of the muscle. Image-based measures 76 were performed using ImageJ (version 1.53a; Bethesda, MD, USA).

77 [Figure 1]

78 Reliability protocol

79 Reliability of US image capture was evaluated for one novice (1 year of practice) and 80 one experienced (13 years of practice) examiner, both using the prone patient positioning as 81 previously described. Each examiner captured two images of the FHL muscle, with a 10-min 82 period between the two image-captures, with participant positioning required for each 83 assessment. Reliability of image-based measurements was evaluated, again, for one 84 experienced and a novice rater, with the same years of experience as the examiners previously 85 described. Measurements were performed in blinded fashion (no identification if images 86 were obtained by the novice or experienced examiner), with images coded using numerical 87 codes.

88 [Figure 1]

89 Reliability of image-based measurements

The intra-rater reliability of image-based measurements of the CSA and thickness of the
 FHL was evaluated for two rater (experienced/novice), and using images obtained from the

92 experienced and novice operators. Inter-rater reliability was evaluated for measures of CSA 93 and thickness using the images obtained during the first imaging assessment from both the 94 experienced and novice examiner. We also evaluated inter-rater reliability of measurement 95 of the FHL CSA and thickness for the experienced and novice examiners for all images 96 obtained at once. For intra-examiner reliability, each examiner repeated measurements of 97 CSA and thickness at a 1-week interval.

98 Statistical analysis

99 Statistical analysis was performed using SPSS (v.22, IBM; Armonk, NY: IBM Corp.), 100 with an α error of 0.05 and a β error of 0.2 for both intra- and inter-examiner/rater reliability. 101 The Shapiro-Wilk test was employed for the normality assumption. A 2-way, mixed-model, 102 consistency-type, intra-class correlation coefficients (ICC) was calculated to test the intra-103 and inter-rater reliability. Reliability was defined as fair (ICC<0.50), moderate 104 (0.50<ICC<0.75), good (0.75<ICC<0.90), or excellent (ICC>0.90) [12]. In addition, the ICC 105 and associated standard deviation (SD) were used to calculate the standard error measurement 106 as a measure of the precision of measurement, as follows: SEM (%) = (SDx $\sqrt{1-ICC}$) x 100.

107 **Results**

108 The age and relevant anthropometric data for the study group are summarized in Table109 1.

110 [Table 1]

Reliability results for image capture and FHL thickness is reported in Table 2. The results showed in this table demonstrate that reliability was excellent, overall, with ICC values ranging between 0.944 to 0.976, with SEM values of 6.8% to 10.0%. There was no difference between the experienced and novice examiner, with inter-examiner ICCs ranging between 0.983 and 0.994, with SEM values of 0.1% to 5.3%.

116 [Table 2]

117 Reliability of image-based measurement of FHL thickness is reported in Table 3. The 118 intra-rater reliability was excellent, with ICCs ranging between 0.954 and 0.972 and SEM 119 values of 1.2% to 9.6%. There was no difference in reliability between the experienced and 120 novice rater, with inter-rater ICCs of 0.950 to 0.980 and SEM values of 6.2% to 8.5%.

121 [Table 3]

Reliability of image capture for CSA is reported in Table 4. The reliability was again excellent, with ICCs of 0.954 to 0.979 and SEM values of 10.8% to 16.5%. There was no difference between the experienced and novice examiner, with inter-rater ICC values of 0.986 to 0.984 and SEM values of 8.9% to 15.0%.

126 [Table 4]

127 Reliability of image-based measurement of CSA is reported in Table 5. The intra-rater

reliability was excellent, with ICCs of 0.961 to 0.986 and SEM values of 9.2% to 14.1%.

129 Again, there was no different between the experienced and novice rater, with inter-rater ICCs

130 of 0.961 to 0.991 and SEM values of 6.9% to 15.1%.

131 [Table 5]

132 **Discussion**

133 Our findings indicate high reliability of image capture of the CSA and thickness of the 134 FHL, as well as for image-based measurements of CSA and thickness This reliability would 135 be independent of the examiner experience. To the authors' knowledge, this is the first study 136 that has evaluated the reliability of both USI capture (positioning) and measurement for the 137 FHL muscle considering the experience of the examiner. Our findings are consistent with 138 previous studies which have reported ICC values >0.90 [7,8], and underscore the feasibility 139 of using USI. Despite the high prevalence of FHL tendinopathy, there is limited evidence of 140 the role of the FHL in foot mechanics, and of the impact of an injury in this muscle [13]. 141 Injuries to the FHL muscle and its tendon are often overlooked. In specific populations, 142 however, appropriate assessment of this muscle is essential, such as in dancers who rely on 143 the FHL for dynamic stability of the foot during movements that require alternation between 144 extreme plantar flexion and dorsiflexion [14]. Dancers are high-performance athletes who 145 are particularly susceptible to lower extremities -specially foot- injuries [15–19]. By 146 demonstrating the reliability of USI of the FHL, this study may offer a novel approach to 147 assess and quantify the injury status of the FHL, as well as providing the image guidance 148 needed for invasive therapies (such as needle insertion) targeting this muscle. The impact of 149 any injury in professional athletes justifies the requirement of improving assessment and 150 treatment techniques and guarantee their reliability [20,21]. Crofts et al. [7] and Mickle et al. 151 [8] placed individuals in a supine position to locate the FHL. However, other studies [6,22],

152 and in particular those targeting invasive therapies such as US-guided percutaneous 153 neuromodulation, have used a prone position for patient placement, with feet unsupported at 154 the end of the plinth. In the present study, prone position was selected, as it has been reported 155 to be more comfortable for the patient, provided greater lower limb stability, and facilitated 156 handling of the probe with one hand and the possible needle with the other [9,10]. Due to 157 these facts, assessing USI reliability in this position was considered to have more implications 158 for potential use in the field of invasive techniques. 159 The authors acknowledge the limitations of this study. Foremost, the small sample size 160 of the study group. The characteristics of the sample, with median age of 21 years, healthy BMI, no previous history of FHL injury and no lower limb impairments, might be not 161 162 representative of the range of patients with FHL tendinopathy. However this results may be 163 useful in future studies in rehabilitation medicine in other populations. Future lines of 164 research might include repeated assessment of reliability in patients with tendinopathy, as 165 well as in athletes with suspected impairments in FHL function. Further research with a

166 higher sample size is needed.

167 Conclusions

USI examination of the FHL muscle is highly reliable for the evaluation of the CSA and thickness of the muscle in healthy participants, not depending on the experience of the examiner. Continued assessment of the reliability of US image capture and image-based measurements of FHL morphometric parameters would be important to extend the importance of USI in clinical practice.

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 Table 1. Sociodemographic data

Data	Total (n = 20)
Age (years)	21.05 ± 2.3
Weight (kg)	56.30 ± 5.6
Height (m)	1.65 ± 0.0
BMI (kg/m ²)	20.46 ± 0.6

Abbreviations: body mass index, BMI

	ICC (95% CI)	SD	SEM
FHL Thickness (cm)			
Intra- Rater (A)			
Experienced Rater	0.957 (0.892- 0.983)	0.435	6.8%
Novice Rater	0.969 (0.922- 0.988)	0.432	7.6%
Intra- Rater (B)			
Experienced Rater	0.963 (0.909- 0.985)	0.426	8.1%
Novice Rater	0.976 (0.938- 0.990)	0.426	6.5%
Intra- Rater (C)			
Experienced Rater	0.964 (0.909- 0.986)*	0.463	8.7%
Novice Rater	0.969 (0.922- 0.988)	0.450	7.9%
Intra- Rater (D)			
Experienced Rater	0.978 (0.945- 0,991)	0.450	6.6%
Novice Rater	0.944 (0.856- 0.978)	0.426	10.0%
Inter- Rater (A)	0.991 (0.976- 0.996)	0.418	0.1%
Inter- Rater (B)	0.983 (0.957- 0.993)	0.412	5.3%
Inter- Rater (C)	0.994 (0.986- 0.998)	0.452	0.1%
Inter- Rater (D)	0.991 (0.977- 0.996)	0.435	0.1%

Table 2. Intra- and inter-rater reliability of imaging for the FHL thickness capturing

	ICC (95% CI)	SD	SEM
FHL thickness (cm)			
Intra- Rater (A)			
Experienced Rater	0.968 (0.920- 0.987)	0.455	8.1%
Novice Rater	0.969 (0.922- 0.988)	0.432	7.6%
Intra- Rater (B)			
Experienced Rater	0.963 (0.909- 0.985)	0.432	8.3%
Novice Rater	0.972 (0.930- 0.989)	0.442	7.3%
Intra- Rater (C)			
Experienced Rater	0.954 (0.885- 0.982)	0.450	9.6%
Novice Rater	0.966 (0.913- 0.986)	0.443	8.1%
Intra- Rater (D)			
Experienced Rater	0.973 (0.931- 0.989)	0.454	1.2%
Novice Rater	0.968 (0.920- 0.987)	0.431	7.7%
Inter- Rater (A)	0.958 (0.897- 0.983)	0.430	7.8%
Inter- Rater (B)	0.967 (0.915- 0.987)	0.415	7.5%
Inter- Rater (C)	0.961 (0.902- 0.985)	0.435	8.5%
Inter- Rater (D)	0.980 (0.950- 0.992)	0.444	6.2%

Table 3. Intra- and inter-rater reliability of imaging for the FHL thickness calculation

	ICC (95% CI)	SD	SEM
FHL CSA (cm ²)			
Intra- Rater (A)			
Experienced Rater	0.967 (0.913- 0.987)	0.733	13.3%
Novice Rater	0.971 (0.928- 0.988)	0.736	12.5%
Intra- Rater (B)			
Experienced Rater	0.979 (0.948- 0.992)	0.749	10.8%
Novice Rater	0.962 (0.904- 0.985)	0.738	14.3%
Intra- Rater (C)			
Experienced Rater	0.967 (0.917- 0.987)	0.694	12.6%
Novice Rater	0.954 (0.882- 0.982)	0.700	16.5%
Intra- Rater (D)			
Experienced Rater	0.970 (0.925- 0.988)	0.744	12.8%
Novice Rater	0.962 (0.907- 0.985)	0.772	15.0%
Inter- Rater (A)	0.984 (0.953- 0.994)	0.710	8.9%
Inter- Rater (B)	0.964 (0.909- 0.986)	0.760	14.4%
Inter- Rater (C)	0.984 (0.960- 0.994)	0.737	9.3%
Inter- Rater (D)	0.965 (0.913- 0.986)	0.732	13.6%

Table 4. Intra- and inter-rater reliability of imaging for the FHL CSA capturing

	ICC (95% CI)	SD	SEM
FHL CSA (cm ²)			
Intra- Rater (A)			
Experienced Rater	0.964 (0.910- 0.986)	0.727	13.7%
Novice Rater	0.964 (0.909- 0.986)	0.723	13.7%
Intra- Rater (B)			
Experienced Rater	0.979 (0.947- 0.991)	0.748	10.8%
Novice Rater	0.972 (0.930- 0.989)	0.757	12.6%
Intra- Rater (C)			
Experienced Rater	0.986 (0.965- 0.994)	0.781	9.2%
Novice Rater	0.961 (0.898- 0.985)	0.714	14.1%
Intra- Rater (D)			
Experienced Rater	0.974 (0.932- 0.990)	0.734	11.8%
Novice Rater	0.966 (0.915- 0.986)	0.769	14.1%
Inter- Rater (A)	0.967 (0.910- 0.988)	0.713	12.9%
Inter- Rater (B)	0.967 (0.918- 0.987)	0.715	12.9%
Inter- Rater (C)	0.991 (0.977- 0.996)	0.735	6.9%
Inter- Rater (D)	0.961 (0.902- 0.985)	0.765	15.1%

Table 5. Intra- and inter-rater reliability of imaging for the FHL CSA calculation.



Ultrasound imaging of the flexor hallucis longus thickness and CSA